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## **Catalytic ferromagnetic gold nanoparticle immunoassay for the detection and differentiation of *Mycobacterium tuberculosis* and *Mycobacterium bovis***

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## 1 1. Introduction

2 Over recent decades, nanomaterials have emerged as promising tools for use in disease  
3 diagnosis [1]. In particular, gold nanoparticles (AuNPs)<sup>1</sup> hold great potential in biosensing  
4 applications because of their ease of functionalisation, high surface-area-to-volume ratio,  
5 unique bio-catalytic abilities, and high stability. AuNPs are employed in a wide range of  
6 biomedical applications including drug-delivery, bio imaging and as optical indicators in lateral  
7 flow assays, whilst their intrinsic peroxidase-like activity has facilitated their use in enzyme-  
8 like mediated biocatalysis of common ELISA substrates including 3,3',5',5'-  
9 tetramethylbenzidine (TMB) [2]. Similarly, magnetic nanoparticles (MNPs) which can be  
10 manipulated and controlled by magnetic fields have been used as catalysts in bioimaging and  
11 biomedicine [3]. MNPs can have dual functionality: their magnetic properties facilitate bio-  
12 separation of target antigens; and they can biocatalyse due to the surface charge associated  
13 catalytic activity conferred by their external surface shell [4]. Combining two different  
14 nanomaterials in a composite NP structure has led to the development of bi-functional NPs  
15 including metallic magnetic iron oxide core – gold shell NPs which are capable of magnetic  
16 separation and are biocompatible [5-7].

17 Tuberculosis (TB) is a disease caused by a group of organisms collectively called the  
18 *Mycobacterium tuberculosis* complex (MTBC). Over one-quarter of the world's population is  
19 infected with MTBC organisms and TB is the leading cause of death worldwide from a single  
20 infectious agent [8]. *Mycobacterium tuberculosis* (MTB) is the primary cause of human  
21 tuberculosis (HTB), however, *Mycobacterium bovis* can also cause TB in humans, referred to  
22 as zoonotic TB (ZTB) [9]. TB disease caused by *M. bovis* is clinically and pathologically  
23 indistinguishable from TB caused by MTB. In addition, both mycobacteria stain as acid fast

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<sup>1</sup> Abbreviations: MTBC, *Mycobacterium tuberculosis* complex; Au-Fe<sub>3</sub>O<sub>4</sub> NPs, Ferromagnetic gold nanoparticles; Fe<sub>3</sub>O<sub>4</sub> NPs, iron oxide nanoparticles; TMB, 3,3',5',5'-tetramethylbenzidine; oxTMB, 3,3',5,5'-tetramethylbenzidine diamine; PBS, Phosphate-buffered saline; NPIDA, nanoparticle based immune detection assay; MTB, *Mycobacterium tuberculosis*; mAb, monoclonal antibody; AuNPs, gold nanoparticles; MNPs, magnetic nanoparticles; ZTB, zoonotic TB; HTB, human tuberculosis; CDC, Centers for Disease Control and Prevention; WHO, World Health Organisation; NAATs, nucleic acid amplification tests; HRP, Horseradish peroxidase; QUBPA-1, MTBC selective polyclonal antibody; QUBMA-1, *M. bovis* selective monoclonal antibody

24 bacilli, are 99.95% similar at the genome level, and have identical 16S rRNA sequences [10].  
25 Differentiation between them is crucial as *M. bovis* is intrinsically resistant to pyrazinamide,  
26 one of the routinely used front-line anti-TB drugs [11]. In high TB burden, low-income  
27 countries, speciation of the causative organisms is rarely undertaken, with the result that when  
28 TB is diagnosed it is assumed to be caused by MTB [12]. Inaccurate diagnosis of ZTB  
29 compromises the efficacy of the treatment regime. This increases the risk of disease  
30 transmission and potentially contributes to the development of antibiotic-resistant TB, resulting  
31 in increased patient morbidities and mortalities [13]. Differential diagnosis of the causative  
32 agent of TB infection is therefore a crucial part of effective disease control plans to: (i)  
33 effectively direct chemotherapy; (ii) facilitate the study of the transmission of mycobacteria  
34 between humans and animals; and (iii) provide more accurate estimations of the scale of ZTB.  
35 The “WHO End TB Strategy” details targets, including an 80% reduction in TB incidence and  
36 95% decrease in TB mortality by 2030, by prioritising patient-centred care strategies,  
37 expanding access to TB treatments for all patients, and calling for diagnosis and treatment of  
38 every person with TB, including ZTB [14]. Therefore, the development of more rapid and easy-  
39 to-use testing approaches for TB detection and speciation are necessary.

40 The gold standard for TB diagnosis is the isolation of MTB by culture, but this is expensive  
41 and time-consuming because of the slow-growing nature of MTBC organisms, which can take  
42 weeks for colonies to grow [15]. In low-income countries, TB diagnosis relies mainly on the  
43 detection of acid-fast bacilli using sputum smear microscopy, but this method is non-specific  
44 and has low sensitivity [16]. Molecular diagnostic assays including Nucleic Acid Amplification  
45 Tests (NAATs) [17], and the WHO endorsed GeneXpert MTB/RIF [18], ELISA [19] and other  
46 immunological tests such as the T-SPOT and QuantiFERON TB IFN- $\gamma$  release assays [20]  
47 offer more sensitive diagnosis than conventional sputum smear microscopy, but suffer from  
48 limitations including requirements for highly skilled personnel, expensive lab equipment and  
49 complex experimental procedures. In addition, none of these tests can differentiate between  
50 MTB and *M. bovis*.

51 The slow-growing pathogenic mycobacteria use a variety of strategies thought to influence  
52 immunopathogenicity. The most important of these tools are secreted proteins, such as the 6-  
53 kDa early secreted antigenic target (ESAT6) [21], the 10-kDa culture filtrate protein (CFP10)  
54 [22], the antigen 85 (Ag85) complex which has a significant role in the virulence of MTB [23],  
55 and MPT64, which is a secreted protein involved in inhibition of macrophage apoptosis [24].  
56 Detection of these proteins can be used to differentiate MTBC from the non-TB producing  
57 mycobacteria, for example, the detection of the MPT64 antigen has been used in various  
58 assays such as the SD Bioline [25], Becton Dickinson MGIT TBc ID test [26] and Tauns Capilia  
59 TB-Neo [27]. These diagnostic tests will identify MTBC, but will not speciate *M. bovis*.  
60 Differentiation of MTB and *M. bovis* has been demonstrated using molecular based methods  
61 which target the *gyrB* (Rv0005) [28] and *hupB* (Rv2986c) [29] gene loci. The former is a two-  
62 step approach using an AuNP-based colorimetric nanoprobe assay for the rapid detection of  
63 MTB complex, and differentiation of *M. bovis* and MTB using *gyrB* (Rv0005) target [28]. On  
64 the other hand, Prabhakar *et al* reported a PCR based assay for distinguishing MTB and *M.*  
65 *bovis* by targeting the *hupB* gene in a single reaction [29]. Three primers—N, M, and S—were  
66 designed and the primer pair N-S amplified the entire *hupB* gene. The C-terminal part of the  
67 gene was selectively amplified by using primers M and S and the size differences in PCR  
68 products were observed to be reliable for distinguishing MTB and *M. bovis* from other MTBC  
69 members. In a previous study, focused in the veterinary context where *M. bovis* predominates,  
70 an *M. bovis* cell wall-associated protein was used to develop a lateral flow device capable of  
71 detecting *M. bovis* [30, 31]. For translation into the human diagnostic context, where both MTB  
72 and *M. bovis* are encountered, a dual test is required that can both identify MTBC and  
73 differentiate *M. bovis*. In this study we produced a novel recombinant antibody to MPT64 and  
74 combined this with previously produced antibodies to develop a low-cost, portable and highly  
75 sensitive NP based assay. The combination of antibodies used resulted in an immunoassay  
76 which could both detect MTBC and differentiate *M. bovis*. This novel assay, when compared  
77 with conventional ELISA using the same antibodies, was found to achieve greater  
78 physiochemical stability, catalytic efficiency, and a shorter time to detection of MTBC

79 organisms. The magnetic capabilities of the functionalised Au-Fe<sub>3</sub>O<sub>4</sub> NP bioconjugates were  
80 exploited during sample preparation, and their intrinsic peroxidase-like catalytic activity  
81 resulted in a semi-quantitative colorimetric detection methodology which directly confirms  
82 presence/absence of MTBC organisms. The developed assay enabled simultaneous  
83 immunological sensing and differentiation of *M. bovis* and MTB. No cross-reactivity was  
84 detected with other non-tuberculosis *Mycobacterium spp.* tested. This novel immunoassay  
85 combined sample preparation and target detection, reduced the number of steps, and  
86 therefore the time required to detection, when compared to traditional ELISA technique.

87

## 88 **2. Methods**

### 89 **2.1 Materials**

90 TMB was purchased from Merck-Millipore, hydrogen peroxide (H<sub>2</sub>O<sub>2</sub>), sodium acetate (Na Ac),  
91 sodium bicarbonate, Tween 20, horseradish Peroxidase (HRP), phosphate-buffered saline  
92 (PBS), sulphuric acid (H<sub>2</sub>SO<sub>4</sub>), dithiothreitol (DTT), Fe (II) and Fe (III) chloride,  
93 tetramethylammonium hydroxide (TMOH), sodium citrate (Na<sub>3</sub>C<sub>6</sub>H<sub>5</sub>O<sub>7</sub>) and tetrachloroauric  
94 acid trihydrate (HAuCl<sub>4</sub> · 3H<sub>2</sub>O) were purchased from Sigma-Aldrich. MPT64 antigen was  
95 purchased from 2BScientific Ltd (Heyford, Oxfordshire, UK). Costar high-binding 96-well  
96 plates were purchased from Corning (New York, USA), 96-well polypropylene microtiter plates  
97 were purchased from Greiner Bio-One (Kremsmünster, Austria), DAKO Goat anti-rabbit and  
98 anti-mouse HRP-conjugated antibodies were purchased from Agilent (CA, USA). Middlebrook  
99 7H9 broth was purchased from Becton Dickinson DIFCO (USA). PD-10 columns were  
100 purchased from GE-Healthcare. MTB H37Rv, *M. bovis* AF2122/97, *M. kansasii* NCTC10268,  
101 *M. avium* subsp. *paratuberculosis* NCTC8578 and *M. bovis* (BCG-strain) NCTC5692 cell  
102 suspensions were produced in-house as detailed previously [30]. Briefly, enumerated bacterial  
103 cultures were centrifuged and washed three times in sterile PBS (0.1M, pH 7.4) before  
104 resuspension in PBS. All mycobacterial cell suspensions were subjected to a 10 kGy dose of  
105 gamma radiation (Gammabeam 650 cobalt irradiator, AFBI, Belfast). After radiation treatment,  
106 samples of each suspension were cultured on Middlebrook 7H10 agar and plates read after

107 56 days, to ensure complete inactivation of all pathogenic mycobacteria before use. Irradiated  
108 bacterial stock cultures diluted in PBS ( $10^6$  CFU mL<sup>-1</sup>) were stored at -80 °C until required.  
109 *Escherichia coli* TG1 DSM6056, and XL1-Blue MRF' strains were cultivated in house.

110

## 111 **2.2 Antibody production**

112 An *M. bovis* mAb and MTBC polyclonal antibodies, labelled QUBMA-1 and QUBPA-1  
113 respectively were sourced from a previous study [32].

114

### 115 **2.2.1 Recombinant antibody selection via phage display**

116 Recombinant antibodies against MPT64 were generated by antibody phage display. The  
117 antibody selection was performed as described previously with modifications and the resultant  
118 monoclonal binders were sequenced and analysed using VBASE2 ([www.vbase2.org](http://www.vbase2.org)) [33-35].

119 (See S1)

120

### 121 **2.2.2 Initial characterisation**

122 Unique single-chain variable fragment (scFv) sequences isolated by antibody-phage display  
123 in Costar high-binding 96-well plates were subcloned into pCSE2.6-mIgG2a-Fc-XP [36] using  
124 *NcoI/NotI* (New England Biolabs, Frankfurt, Germany). For production, the transfected  
125 EXPI293F cells were cultured in chemically defined medium F17 (Thermo Fisher Scientific)  
126 supplemented with 0.1% pluronic F68 (PAN-Biotech, Aidenbach, Germany) and 7.5 mM L-  
127 glutamine (Merck). A subsequent protein A purification was performed as described previously  
128 [37].

129 The purified scFv-Fc antibodies were initially characterised by indirect ELISA, performed by  
130 coating 50 ng per well of MPT64 diluted in PBS. The recombinant antibodies were 10-fold  
131 serially diluted in 2% Modified PBS-T (2% (w/v) milk powder in PBS; 0.05% Tween20) (MPBS-  
132 T) from 10 µg mL<sup>-1</sup> to 3.16 ng mL<sup>-1</sup>, and 100 µL per well of each dilution added. The secondary  
133 antibody, goat anti-mouse HRP, was added and the reaction developed with TMB solution  
134 and read at 450 nm with a 620 nm reference. As a negative control, a non-related His-tagged

135 recombinant protein produced in *E. coli* was coated on a plate and tested in the same way.  
136 Absorbance values were used to calculate EC<sub>50</sub> value using GraphPad software (Prism, v  
137 5.01).

138

### 139 **2.3 Synthesis of Fe<sub>3</sub>O<sub>4</sub> and Au-Fe<sub>3</sub>O<sub>4</sub> composite NPs**

140 The method of Pham *et al* was used to synthesise Fe<sub>3</sub>O<sub>4</sub> NPs [38]. Briefly, ddH<sub>2</sub>O (20 mL) was  
141 degassed by sonicating for 30 min in a triple neck flask before purging with N<sub>2</sub> gas for 20 min.  
142 Fe (III) chloride (4.6g) and Fe (II) chloride (1.7g) were added to HCl (100 mM) and stirred  
143 vigorously until fully dissolved before adding NaOH (2 M, 20 mL) dropwise yielding a dark  
144 black magnetic precipitate. The precipitate was collected using a 3,000 G magnet and washed  
145 in ddH<sub>2</sub>O before resuspension in tetramethylammonium hydroxide (TMOH) (0.1 M, 10 mL).  
146 Iron oxide NPs were obtained by further washing and dissolving in nitric acid (HNO<sub>3</sub>) (0.01 M,  
147 10 mL) with stirring until the solution produced a brown colour. The synthesised iron oxide  
148 NPs were washed in ddH<sub>2</sub>O before resuspending in TMOH (0.1 M, 10 mL).

149 A modified version of the Turkevich method for AuNP production in trisodium citrate [39] was  
150 used to synthesise gold-iron oxide nanocomposites. Sodium citrate (0.1 M, 10 mL) and  
151 synthesised iron oxide NPs (1 mL) were boiled with stirring for 10 min, before addition of  
152 HAuCl<sub>4</sub>·4H<sub>2</sub>O (1 mM, 1 mL) to produce iron oxide-gold composite NPs. A red-wine colour  
153 developed within 10 min and the resultant composite NPs were magnetically collected and  
154 washed three times in ddH<sub>2</sub>O (10 mL), and once in sodium citrate (0.1 M, 10 mL), before  
155 storing at 4 °C until use. The resultant composite NPs were standardised to OD<sub>550</sub> = 1.0 before  
156 use.

157

### 158 **2.4 Characterisation of Au-Fe<sub>3</sub>O<sub>4</sub> NPs**

159 The peroxidase activity of the Au-Fe<sub>3</sub>O<sub>4</sub> NPs was assessed at a range of H<sub>2</sub>O<sub>2</sub> concentrations,  
160 pH and temperatures. Au-Fe<sub>3</sub>O<sub>4</sub> NPs (0.1 nM, OD<sub>550</sub> = 1) and HRP (3 nM) solutions were  
161 prepared in sodium acetate buffer (2 mM, pH 5, 1 mL). The peroxidase activity of Au-Fe<sub>3</sub>O<sub>4</sub>  
162 NPs and HRP was compared by incubating 1 mL of each Au-Fe<sub>3</sub>O<sub>4</sub> NP solution and HRP in

163 sodium acetate buffer with TMB (0.65 mM, 100  $\mu$ L) for 2 hrs at 37  $^{\circ}$ C. The peroxidase activity  
164 was measured at a range of: (i)  $\text{H}_2\text{O}_2$  concentrations, by preparing solutions of Au- $\text{Fe}_3\text{O}_4$  NP  
165 (1 mL) at final  $\text{H}_2\text{O}_2$  concentrations of 0, 1, 2, 3, 4, 6, 8 and 10% (v/v), (ii) pH, by preparation  
166 of Au- $\text{Fe}_3\text{O}_4$  NP solutions (1 mL) with pH adjusted to 2, 3, 4, 5, 6, 7, 8 and 9 and, (iii)  
167 temperatures, by varying the incubation temperature of five Au- $\text{Fe}_3\text{O}_4$  NP solutions (1 mL) to  
168 20, 30, 40, 55 and 65  $^{\circ}$ C. TMB substrate oxidation absorbance readings were measured using  
169 a Safire 96-well ELISA plate reader (Tecan, Switzerland) at 370 nm immediately after  
170 incubation.

171 TMB oxidation was demonstrated by preparing two solutions of 0.65 mM TMB / 8% (v/v)  $\text{H}_2\text{O}_2$   
172 in sodium acetate buffer (2 mM, pH 5, 1 mL) in semi-micro cuvettes. Au- $\text{Fe}_3\text{O}_4$  NPs (0.1 nM,  
173 10  $\mu$ L) were added to one cuvette and the TMB substrate oxidation profile recorded in both  
174 cuvettes using a spectrophotometer.

175 To determine if the relative peroxidase activity being measured was due to intact Au- $\text{Fe}_3\text{O}_4$   
176 NPs, two solutions of Au- $\text{Fe}_3\text{O}_4$  NPs (0.1 nM) in sodium acetate buffer (2 mM, pH 5, 1 mL)  
177 were prepared. A 3000 G permanent magnet was used to remove the Au- $\text{Fe}_3\text{O}_4$  NPs from one  
178 solution. One hundred  $\mu$ L of 0.65 mM TMB / 8% (v/v)  $\text{H}_2\text{O}_2$  was added to both and the relative  
179 peroxidase activity of each solution was measured continuously for 10 min at 370 nm using a  
180 spectrophotometer.

181

## 182 **2.5 Characterisation of NP structure**

183 Transmission electron microscopy images of Au- $\text{Fe}_3\text{O}_4$ , Au and  $\text{Fe}_3\text{O}_4$  NPs were obtained  
184 using a Joel JEM-1400 Plus Transmission Electron Microscope 120 kV. Samples were  
185 prepared on carbon-nickel grids in 50% (v/v) ethanol. UV-Vis analysis of particles was  
186 achieved using a Cary 60 spectrophotometer (Agilent Technologies, USA). Dynamic Light  
187 Scattering (DLS) particle size and zeta potential measurements were obtained using a  
188 Malvern Zetasizer Nano ZS (Malvern Panalytical, Worcestershire, UK)

189

## 190 **2.6 Au- $\text{Fe}_3\text{O}_4$ NP functionalisation and characterisation**



191 QUBPA-1 was used as the capture antibody in the assay. Au-Fe<sub>3</sub>O<sub>4</sub> NPs were bio-  
192 functionalised by direct coupling of QUBPA-1 using DTT [40-42]. Briefly, DTT (0.35 mg) was  
193 added per 1 mL of antibody (0.2 mg mL<sup>-1</sup>) diluted in PBS EDTA (2 mM, pH 7.4, 1 mL) buffer  
194 solution, and incubated on a rotator for 30 min at room temperature. Excess reactants were  
195 removed by separation in PD-10 columns using PBS EDTA washing buffer before collecting  
196 eight successive eluted antibody fractions (0.5 mL). Antibody fraction concentrations were  
197 measured at 280 nm on a NanoDrop 8000 (Thermoscientific, UK) and the peak antibody  
198 fraction (0.1 mg mL<sup>-1</sup>) was added to 1 mL of Au-Fe<sub>3</sub>O<sub>4</sub> NPs (OD<sub>550</sub> = 1) and left for 16 h at  
199 room temperature to enable conjugation. Resultant antibody Au-Fe<sub>3</sub>O<sub>4</sub> NP bioconjugates were  
200 washed three times in PBS-0.05% Tween-20 buffer (pH 7.4) (PBS-T) and stored at 2 – 8 °C.  
201 Relative peroxidase activity of uncoated and antibody functionalised Au-Fe<sub>3</sub>O<sub>4</sub> NPs was  
202 determined by preparing solutions of uncoated Au-Fe<sub>3</sub>O<sub>4</sub> NPs and antibody functionalised Au-  
203 Fe<sub>3</sub>O<sub>4</sub> NPs (0.1 nM) in sodium acetate buffer (2 mM, pH 5, 1 mL). TMB (0.65 mM) / 8% (v/v)  
204 H<sub>2</sub>O<sub>2</sub> (100 µL) was added to each sample and the relative peroxidase activity of each solution  
205 measured continuously for 10 min at 370 nm using a spectrophotometer.

206

## 207 **2.7 Immunoassays**

### 208 **2.7.1 NP-based Immune Detection Assay (NPIDA)**

209 Nunc Maxisorp™ plates were coated with detector antibodies, either recombinant antibody or  
210 QUBMA-1 (10 µg mL<sup>-1</sup>, 100 µL), diluted in bicarbonate buffer (0.1 M, pH 9.4), and incubated  
211 for 16 h at 4 °C. After incubation, they were washed five times with PBS-T wash buffer before  
212 blocking with assay buffer (PBS-T/BSA (1% w/v)), (200 µL per well) for 2 h at 37 °C with  
213 shaking. The solution was then discarded.

214 Concurrently, Au-Fe<sub>3</sub>O<sub>4</sub> NP-antibody bioconjugates (100 µL), coated with the capture  
215 antibody, were incubated with whole cells of either MTB or *M. bovis* (1 x 10<sup>5</sup> CFU mL<sup>-1</sup>) diluted  
216 in assay buffer (1 mL) for 16 h at 37 °C in 1.5 mL tubes. Negative control samples were  
217 prepared by incubating Au-Fe<sub>3</sub>O<sub>4</sub> NP-antibody bioconjugates (100 µL) with assay buffer only.  
218 After incubation with target cells, Au-Fe<sub>3</sub>O<sub>4</sub> NP-antibody bioconjugates were washed three

219 times in PBS-T/SDS (0.001 % w/v), collected using a magnetic stand between each wash.  
220 The washed bioconjugate was then added to the antibody coated, blocked plate, and  
221 incubated for 2 h at 37 °C with shaking. The plates were washed five times using PBS-T before  
222 adding TMB substrate (100 µL per well). The colour was left to develop for 30 min, stop  
223 solution (2.5 M H<sub>2</sub>SO<sub>4</sub>, 25 µL per well) added, and the plate read at 450 nm using a microplate  
224 reader.

225

### 226 **2.7.2 Conventional sandwich ELISA**

227 For comparison with conventional sandwich ELISA the same method was followed as detailed  
228 previously for the NPIDA with minor changes. Nunc Maxisorp™ plates were coated as before.  
229 After removing blocking buffer and washing plates five times with PBS-T, each target bacterial  
230 culture (1 x 10<sup>5</sup> CFU mL<sup>-1</sup>, 100 µL per well) diluted in assay buffer, was added directly to the  
231 wells and incubated for 2 h at 37 °C with shaking. Plates were washed five times with PBS-T,  
232 the detector antibody (either QUBPA-1, GSM237-G8 or QUBMA-1) (10 µg mL<sup>-1</sup>, 100 µL per  
233 well) added, and the plates incubated for 1.5 h at 37 °C. Plates were washed five times with  
234 PBS-T and the appropriate secondary antibody, (DAKO anti-mouse/ rabbit HRP conjugate  
235 antibody) (0.25 µg mL<sup>-1</sup>, 100 µL per well), diluted in assay buffer added, and incubated for 1 h  
236 at 37 °C with shaking. Plates were then washed 5 times in PBS-T before adding TMB substrate  
237 (100 µL per well). The plate was left for 30 mins before adding stop solution, (2.5 M H<sub>2</sub>SO<sub>4</sub>,  
238 25 µL per well) and the absorbance read at 450 nm using a microplate reader.

239

### 240 **2.7.3 Limits of Detection of developed assays**

241 The 50% limit of detection (LOD<sub>50%</sub>) for both the NPIDA and the conventional sandwich ELISA  
242 were determined both in assay buffer and in BACTEC™ MGIT™ TB media (7H9 Middlebrook  
243 broth/10 % OADC) using the assay procedures detailed above. A tenfold dilution series  
244 containing 10<sup>5</sup>, 10<sup>4</sup>, 10<sup>3</sup>, 10<sup>2</sup>, 10<sup>1</sup> and 0 CFU mL<sup>-1</sup> of both MTB and *M. bovis* whole cells was  
245 prepared in assay buffer and in BACTEC™ MGIT™ TB media. In the NPIDA, each cell dilution  
246 (1 mL) was incubated with Au-Fe<sub>3</sub>O<sub>4</sub> NP-antibody bioconjugates, whereas in the conventional

247 sandwich ELISA each cell dilution was added to a previously coated 96-well plate  
248 (recombinant antibody or QUBMA-1) after the blocking step. All samples were prepared in  
249 triplicate, all experiments were repeated three times resulting in a total of 9 replicate values at  
250 6 dilutions. The LOD<sub>50%</sub> was determined using the generalized Spearman-Kärber LOD<sub>50%</sub>  
251 calculation for 6-level spiking protocols [43].

252

### 253 **3. Results and Discussion**

254 In this study, a novel ferromagnetic gold NP immunoassay was developed and evaluated for  
255 the detection and differentiation of MTB and *M. bovis*, the main causative agents of TB in  
256 humans. A unique recombinant monoclonal antibody to a key MTBC protein was generated  
257 and used in conjunction with a panel of pre-existing antibodies to cell surface and secreted  
258 antigens of MTB and *M. bovis*, to develop the assay. Au-Fe<sub>3</sub>O<sub>4</sub> NP bioconjugates were  
259 prepared by direct coupling of antibodies to Au-Fe<sub>3</sub>O<sub>4</sub> NPs which were then used to develop  
260 the NPIDA. The NPIDA was capable of sensitive detection and differentiation of MTB and *M.*  
261 *bovis* cells.

262

#### 263 **3.1 Au-Fe<sub>3</sub>O<sub>4</sub> NP composition and peroxidase-like activity**

264 Fe<sub>3</sub>O<sub>4</sub> NPs were synthesised first, and subsequently alloyed with Au to form Au-Fe<sub>3</sub>O<sub>4</sub> NPs  
265 following a modified version of the established sodium citrate seeding method by Brown *et al*  
266 [44]. As seen in **Figure 1a**, Fe<sub>3</sub>O<sub>4</sub> NPs do not exhibit any peaks from 400-800 nm (green line),  
267 and AuNPs possess a characteristic plasmonic peak at 517 nm (solid line). The formation of  
268 Au-Fe<sub>3</sub>O<sub>4</sub> NPs was confirmed by the UV-Vis spectroscopy with the presence of a distinct peak  
269 at 550 nm corresponding to the surface plasmonic peak of the Au nanomaterial. The shift in  
270 peak wavelength (from 517 to 550 nm) corresponded to an increase in NP diameter. This has  
271 previously been observed during Au-Fe<sub>3</sub>O<sub>4</sub> NP synthesis, wherein successful assembly of Au  
272 with the Fe<sub>3</sub>O<sub>4</sub> NPs led to a similar shift in peak wavelength [45]. The magnetic capabilities of  
273 Fe<sub>3</sub>O<sub>4</sub> NPs and Au-Fe<sub>3</sub>O<sub>4</sub> NPs were demonstrated by collection using a 3000 G permanent  
274 magnet, resulting in a phase separation in both the Fe<sub>3</sub>O<sub>4</sub> NP and Au-Fe<sub>3</sub>O<sub>4</sub> NP solutions after

275 the ferromagnetic NPs had migrated towards the permanent magnet (**Figure 1b**). The  
276 demonstration of both magnetism and plasmonic properties unambiguously confirms the  
277 successful production of Au-Fe<sub>3</sub>O<sub>4</sub> NPs. TEM images further revealed that the multiple-faced  
278 Fe<sub>3</sub>O<sub>4</sub> NPs and the Au-Fe<sub>3</sub>O<sub>4</sub> NPs composites have estimated diameters ranging from 15 –  
279 50 nm (**Figure 1c**). Pham *et al* also reported similar observations during Au-Fe<sub>3</sub>O<sub>4</sub> NP  
280 synthesis, noting the formation of spherical-like, multiple-faced Au-Fe oxide NPs following the  
281 reduction of Au<sup>3+</sup> ions onto ‘jagged’ Fe oxide NPs [38]. DLS measurements were taken for  
282 Fe<sub>3</sub>O<sub>4</sub> NPs and Au-Fe<sub>3</sub>O<sub>4</sub> NPs in liquid phase and revealed larger nanoparticle hydrodynamic  
283 diameters, i.e. 153.7 and 300.6 nm, respectively (**Figure S1a**). The discrepancy between the  
284 estimated diameters obtained by TEM and by DLS is thought to be as a result of the magnetic  
285 nature of the iron oxide component of the nanomaterials which causes them to magnetise and  
286 agglomerate into larger particle clusters, an effect which has also been reported by other  
287 groups during analysis of Au-Fe<sub>3</sub>O<sub>4</sub> NPs [46, 47]. In fact, the hydrodynamic diameter of the  
288 same Au-Fe<sub>3</sub>O<sub>4</sub> NPs increased from ca. 300 nm to 800 nm as a function of time (**Fig S1b**) due  
289 to the magnetised susceptibility of the Au-Fe<sub>3</sub>O<sub>4</sub> NPs. The agglomeration causing apparent  
290 increased particle size (**Fig S1c**) can be reversed by applying a prompt sonication (data not  
291 shown).

292

### 293 **3.2 Functionalisation of the Au-Fe<sub>3</sub>O<sub>4</sub> NPs forms the basis of a novel NP-based** 294 **immunoassay**

295 The intrinsic peroxidase-mimicking ability of Au-Fe<sub>3</sub>O<sub>4</sub> NPs enables them to perform as an  
296 artificial-HRP nanozyme capable of oxidising TMB in the presence of H<sub>2</sub>O<sub>2</sub>. The catalytic  
297 efficiency of enzyme catalysts such as HRP and inorganic nanozymes, like Au-Fe<sub>3</sub>O<sub>4</sub> NPs, is  
298 dependent on environmental conditions including temperature, pH and H<sub>2</sub>O<sub>2</sub> concentration.  
299 Inorganic nanomaterials, such as Au-Fe<sub>3</sub>O<sub>4</sub> NPs, are predicted to have greater thermal, pH  
300 and chemical tolerances than organic enzymes like HRP [48]. To assess this hypothesis,  
301 consecutive experiments were set up, measuring TMB oxidation at fixed concentrations of 3  
302 nM HRP and 0.1 nM Au-Fe<sub>3</sub>O<sub>4</sub> NP respectively, under varying environmental conditions

303 including H<sub>2</sub>O<sub>2</sub> concentration, temperature and pH. Au-Fe<sub>3</sub>O<sub>4</sub> NPs were found to require H<sub>2</sub>O<sub>2</sub>  
304 concentrations of 8 % (v/v) to achieve maximal activity and were inhibited at lower/ higher  
305 concentrations, whereas, for HRP the optimal H<sub>2</sub>O<sub>2</sub> concentration was determined to be 0.5  
306 % (v/v) which decreased rapidly at increasing concentrations (**Figure 2a**). Both Au-Fe<sub>3</sub>O<sub>4</sub> NP  
307 and HRP exhibited optimal catalytic activity around pH 5, however the Au-Fe<sub>3</sub>O<sub>4</sub> NPs  
308 demonstrated greater peroxidase activity over a broader range of pH values, pH 4 to pH 7,  
309 compared to HRP (**Figure 2b**). At temperatures over 37 °C, HRP catalytic activity was 25%  
310 lower than Au-Fe<sub>3</sub>O<sub>4</sub> NPs (**Figure 2c**). The maximum point of each curve was set as 100%  
311 relative activity and optimal conditions for TMB oxidation were determined to be 8% H<sub>2</sub>O<sub>2</sub>, 37  
312 °C at pH 5. The oxidation of TMB (0.65 mM) by Au-Fe<sub>3</sub>O<sub>4</sub> NPs in the presence of 8% H<sub>2</sub>O<sub>2</sub>  
313 produces a blue oxidation product, whilst in the absence of Au-Fe<sub>3</sub>O<sub>4</sub> NPs, TMB is unoxidised  
314 and the solution remains colourless (**Figure 2d**). TMB oxidation produces two major peaks  
315 observed at 370 nm and 652 nm by Au-Fe<sub>3</sub>O<sub>4</sub> NPs corresponding to the formation of blue,  
316 oxidised TMB product (**Figure 2e**) [49]. Previous studies have highlighted the peroxidase-like  
317 activity of leached Fe (II) and Fe (III) ions in acidic solution [7, 48]. Therefore, to confirm that  
318 the observed peroxidase-like activity is due to intact Au-Fe<sub>3</sub>O<sub>4</sub> NPs, and not leached iron ions,  
319 a 3000G magnet was used to remove Au-Fe<sub>3</sub>O<sub>4</sub> NPs and the remaining solution analysed  
320 along with the original preparation of Au-Fe<sub>3</sub>O<sub>4</sub> NPs. TMB was added to each sample and  
321 relative peroxidase activity of both solutions measured at 370 nm for 10 min. In the presence  
322 of Au-Fe<sub>3</sub>O<sub>4</sub> NPs, TMB oxidation increased steadily over 10 min, producing the blue coloured  
323 oxidised TMB product, whereas in samples with Au-Fe<sub>3</sub>O<sub>4</sub> NPs removed (No-NP), TMB  
324 remained unoxidised and the sample remained colourless (**Figure 2f**). The peroxidase-like  
325 activity was therefore due to intact Au-Fe<sub>3</sub>O<sub>4</sub> NPs which represent potential candidates for  
326 oxidation of TMB in environmental conditions unsuitable for conventional organic enzymes  
327 like HRP.

328 Modification of NPs with small ligands and metal ions has often been reported to result in a  
329 decrease of catalytic activity. For example, Tao *et al* [50], reported a decrease in peroxidase-  
330 like activity of AuNPs as a result of hindrance by the small ligand biomolecule dopamine.

331 Likewise, antibodies may cause a decrease in peroxidase activity by surface hindrance. In this  
332 study, we compared the relative peroxidase activity of uncoated and antibody-functionalised  
333 Au-Fe<sub>3</sub>O<sub>4</sub> NPs (OD<sub>550</sub> = 1) (**Figure 3**). After 10 mins the rate of formation of blue oxidised TMB  
334 product was reduced by approximately 25 % following surface attachment of the antibody to  
335 the Au-Fe<sub>3</sub>O<sub>4</sub> NPs (uncoated Au-Fe<sub>3</sub>O<sub>4</sub> NPs Abs = 1.04 OD<sub>370</sub>, antibody-functionalised Au-  
336 Fe<sub>3</sub>O<sub>4</sub> NP Abs = 0.72 OD<sub>370</sub>) (**Figure 3a**). However, despite this suppression of catalytic  
337 activity the resultant bioconjugate could still be used for direct sample sensing. The UV-Vis  
338 spectral analysis for TMB oxidation showed a decrease in peak absorbance at 370 nm and  
339 652 nm, corresponding to the suppression of TMB oxidation by the antibody functionalised  
340 Au-Fe<sub>3</sub>O<sub>4</sub> NPs (**Figure 3b**).

341 Having characterised the activity of the individual constituents they were then combined with  
342 antibodies to develop the NPIDA. In the first step the antibody-functionalised Au-Fe<sub>3</sub>O<sub>4</sub> NP  
343 bioconjugate was incubated with target cells. After collecting the Au-Fe<sub>3</sub>O<sub>4</sub> NP bioconjugate-  
344 cell complex on a magnet, the bioconjugate-cell complex was added to wells pre-coated with  
345 detector antibody then washed after incubation to remove unbound bioconjugate-cell  
346 complexes. TMB substrate was added to each well and the peroxidase-mimicking activity of  
347 any captured Au-Fe<sub>3</sub>O<sub>4</sub> NP bioconjugate produced a blue coloured oxidation product in the  
348 presence of H<sub>2</sub>O<sub>2</sub>. The absorbance intensity of the oxidised TMB product was proportional to  
349 the amount of Au-Fe<sub>3</sub>O<sub>4</sub> NP bioconjugate-cell complexes present after binding to the detector  
350 antibody. The more Au-Fe<sub>3</sub>O<sub>4</sub> NP bioconjugate-cell complexes bound to the detector antibody,  
351 the greater the overall intensity of TMB oxidation signal produced. A schematic of the NPIDA  
352 is detailed in **Figure 4**. The NPIDA was then compared with conventional sandwich ELISA  
353 wherein plates were coated with capture antibody before adding target cells, followed by a  
354 secondary (detector) antibody, whose presence is then detected using an HRP conjugated  
355 anti-species antibody in a two-step consecutive process.

356

357 **3.3 Discrete combinations of monoclonal and polyclonal antibodies enabled speciation**  
358 **of MTB and M. bovis**

359 A total of 10 phage display derived recombinant binders were selected for investigation,  
360 produced as scFv-Fc antibodies, and initially tested by indirect ELISA. After titration using the  
361 MPT64 antigen as target and determination of cross reactivity, a single recombinant antibody  
362 (GSM237-G8) was chosen for further experiments (**Figure 5**).

363 Approaches which combine immunomagnetic separation with sandwich ELISA format  
364 immunoassays are more sensitive than indirect ELISA as they facilitate enrichment of groups  
365 of target cells in samples of low concentration, such as the detection and enrichment of  
366 bacterial species in wastewater samples [51]. To select the optimal combination of antibodies  
367 for detection of each organism in the NPIDA, various pairs of target-binding capture and  
368 detection antibodies were screened by conventional sandwich ELISA (**Figure S2**). Each  
369 antibody combination was evaluated for optimal detection of MTB or *M. bovis* cells. In the  
370 conventional sandwich ELISA, the capture antibody selected for MTB was GSM237-G8,  
371 QUBMA-1 was selected for capture of *M. bovis* cells, and QUBPA-1 was selected as the  
372 detector antibody for both mycobacteria (**Figure S3**). In the NPIDA the detector antibody  
373 selected for MTB cell detection was GSM237-G8, QUBMA-1 was selected for detection of *M.*  
374 *bovis* cells, and QUBPA-1 was the capture antibody selected for both mycobacteria (**Figure**  
375 **S4**). Au-Fe<sub>3</sub>O<sub>4</sub> NPs were functionalised with QUBPA-1 by DTT reduction. This method avoids  
376 modification of the antigen binding sites by reducing IgG antibody disulphide bonds within the  
377 antibody hinge region, enabling resultant thiol groups to anchor antibodies to the gold shell of  
378 the Au-Fe<sub>3</sub>O<sub>4</sub> NPs [39-44, 52]. To confirm successful immobilisation of the antibody to the  
379 functionalised Au-Fe<sub>3</sub>O<sub>4</sub> NPs and assess target specificity of the novel NPIDA, a cross-  
380 reactivity analysis was carried out by NPIDA and the results compared with conventional  
381 ELISA. In the NPIDA the NP bioconjugate was incubated overnight with MTB, *M. bovis* and  
382 *M. bovis* BCG-strain (NCTC5692) and two non-tuberculosis mycobacterial species, *M.*  
383 *kansasii* (NCTC10268) and *M. avium* subsp. *paratuberculosis* (MAP) (NCTC8578), whilst in  
384 parallel, GSM237-G8 antibody and QUBMA-1 were coated onto separate 96-well Nunc  
385 Maxisorp™ plates, and the assay carried out as detailed previously (2.7.1). The results  
386 showed that when GSM237-G8 was used as the detector antibody the mean OD<sub>450</sub> of Au-

387 Fe<sub>3</sub>O<sub>4</sub> NP QUBPA-1 with MTB ( $1\pm 0.038$ ) was significantly higher ( $P < 0.001$ ) than the mean  
388 value for *M. bovis* ( $0.33\pm 0.014$ ), confirming that the antibody had been successfully  
389 conjugated to the Au-Fe<sub>3</sub>O<sub>4</sub> NP and the assay was more selective for MTB than *M. bovis*  
390 (**Figure 6a**).

391 Other research groups have reported a decrease of binding affinity resulting from conjugation  
392 of antibodies to labels such as fluorophores/ AuNPs and have indicated that such 'trade-offs'  
393 may be necessary during attachment of binders [53]. However, in the present study, target  
394 selectivity of the antibody was retained following conjugation to the Au-Fe<sub>3</sub>O<sub>4</sub> NP by DTT  
395 reduction, which has also been found by Ji *et al* [41]. A comparison between conventional  
396 sandwich ELISA and Au-Fe<sub>3</sub>O<sub>4</sub> NP QUBPA-1 bioconjugate with QUBMA-1 coated onto 96-  
397 well plates indicated the bioconjugate had retained its selectivity for *M. bovis* and the mean  
398 OD<sub>450</sub> of Au-Fe<sub>3</sub>O<sub>4</sub> NP QUBPA-1 bioconjugate with *M. bovis* ( $1\pm 0.005$ ) was found to be  
399 significantly higher ( $P < 0.001$ ) than the mean value for MTB ( $0.28\pm 0.022$ ) (**Figure 6b**). The  
400 novel NPIDA based assays for MTB and *M. bovis* can be run simultaneously using QUBPA-1  
401 as the capture antibody and Nunc plates which are coated on one half with GSM237-G8 to  
402 detect MTBC, and on the other half with QUBMA-1 to detect *M. bovis*. As such the one  
403 immunoassay can be used to simultaneously detect and differentiate *M. bovis* from MTB.

404 The BD BACTEC™ MGIT™ is a liquid media system commonly used for cultivation of  
405 mycobacteria. To determine the potential suitability of the novel NPIDA for detection of MTB  
406 and *M. bovis* in culture media, and to compare the LOD<sub>50%</sub> of each pathogen in buffer and  
407 broth using both immunoassay formats, a tenfold dilution series of MTB and *M. bovis* ranging  
408 from  $1 \times 10^5$  CFU mL<sup>-1</sup> to 0 CFU mL<sup>-1</sup> was prepared in assay buffer and in MGIT media. The  
409 NPIDAs and conventional ELISAs were carried out as detailed previously and the results for  
410 each assay illustrated in **Table 1**. The results confirm that both the MTB and *M. bovis* ELISAs  
411 and NPIDAs have comparable LOD<sub>50%</sub> values, and therefore similar sensitivities, in both buffer  
412 and BD BACTEC™ MGIT™ and indicate minimal matrix effects when the assays were  
413 transferred from buffer into culture media. The novel NPIDA assay could be applied following



414 culture of samples and used to replace conventional Ziehl-Neelsen staining and subsequent  
415 molecular identification when a TB BACTEC™ MGIT™ culture indicates positive.

416

#### 417 **4. Conclusion**

418 This study reports the synthesis of Au-Fe<sub>3</sub>O<sub>4</sub> NPs by combining citrate capped AuNPs and co-  
419 precipitated Fe<sub>3</sub>O<sub>4</sub> NPs. The physicochemical properties of the resultant iron oxide-gold  
420 composite NPs were characterised, and their magnetic separation capabilities and intrinsic  
421 peroxidase-like activity demonstrated. Functionalisation of the Au-Fe<sub>3</sub>O<sub>4</sub> NPs with MTB and  
422 *M. bovis* selective antibodies led to the development of a NP-based immune-detection assay  
423 capable of detection and differentiating MTB and *M. bovis*. To the best of our knowledge this  
424 assay represents the first immune based diagnostic test capable of differentiating between  
425 MTB and *M. bovis*. The NPIDA demonstrated comparable levels of sensitivity and catalytic  
426 activity to conventional ELISA but enhanced pH and temperature stabilities compared with  
427 conventional HRP. The magnetic capability of the iron cores was exploited in sample  
428 preparation and the intrinsic peroxidase-mimicking ability of NPs negated the requirement for  
429 a time-consuming antibody incubation step required during conventional ELISA. The NPIDA  
430 is a low cost tool which can identify MTB, and speciate *M. bovis*, and therefore has the  
431 potential to more quickly direct patient treatment regimens thus improving the efficacy of  
432 treatments and reducing the emergence of TB drug-resistant phenotypes, particularly in high  
433 TB burden countries. The methodology described in this research should not be limited to the  
434 detection of MTBC but could be employed in other biosensing applications by combining Au-  
435 Fe<sub>3</sub>O<sub>4</sub> NPs with alternative binders specific for metabolites or pathogens of biological interest.  
436 Future investigations will include extended cross reactivity studies and the application of the  
437 TB NIPDA directly with sputum samples.

438

#### 439 **Conflicts of interest**

440 There are no conflicts to declare

441

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446

#### 447 **Associated Supplementary Material**

448 Recombinant antibody selection via phage display; DLS measurement of Fe<sub>3</sub>O<sub>4</sub> NPs and Au-  
449 Fe<sub>3</sub>O<sub>4</sub> NPs in water; Optimisation of antibody pair combinations with QUBPA-1 detection  
450 antibody; Schematic representation of the conventional sandwich ELISA with MTB and *M.*  
451 *bovis*; Schematic representation of the NPIDA with MTB and *M. bovis*.

452

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